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Connectivity-based parcellation: critique & implications

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Abstract

Regional specialization and functional integration are often viewed as two fundamental principles of human brain organization. They are closely intertwined because each functionally specialized brain region is probably characterized by a distinct set of long-range connections. This notion has prompted the quickly developing family of connectivity-based parcellation (CBP) methods in neuroimaging research. CBP assumes that there is a latent structure of parcels in a region of interest (ROI). First, connectivity strengths are computed to other parts of the brain for each voxel/vertex within the ROI. These features are then used to identify functionally distinct groups of ROI voxels/vertices. CBP enjoys increasing popularity for the in-vivo mapping of regional specialization in the human brain. Due to the requirements of different applications and datasets, CBP has diverged into a heterogeneous family of methods. This broad overview critically discusses the current state as well as the commonalities and idiosyncrasies of the main CBP methods. We target frequent concerns faced by novices and veterans to provide a reference for the investigation and review of CBP studies.

Keywords

Brain parcellation, clustering, resting-state correlations, diffusion MRI, data-driven, statistical learning, statistical inference, double dipping

Introduction

The human brain is commonly assumed to be organized in distinct modules (Brodmann, 1909; Vogt and Vogt, 1919). These could be described according to structure, connectivity, and function. *Cortical areas* can be conceptualized as patches of the brain that differ from their neighbors in terms of their microarchitecture (e.g., cyto-, myelo- and receptorarchitecture), connectivity (i.e., set of input and output connections), and function (e.g., lesion-induced behavior or electrophysiological responses) (Felleman et al., 1991; Van Essen, 1985). The conjunction of i) input and output *connectivity* of a cortical area and ii) its local *infrastructure* is thought to crucially determine what classes of computational problems (i.e., *function*) it can solve (Scannel et al., 1995; Mesulam 1998; Passingham et al., 2002; Saygin et al., 2012).

The correspondence between a cortical area and its axonal connectivity fingerprint has prompted connectivity-based parcellation (CBP) approaches (Behrens and Johansen-Berg, 2005; Wiegell et al., 2003). Capitalizing on the distinct connections of each area (Passingham et al., 2002), CBP divides a region of interest (ROI, i.e., a volume- or surface-based topographical definition) into distinct subregions. The key idea is to first compute a connectivity profile for each individual voxel or vertex in the ROI. The voxel/vertex-wise connectivity profiles are then used to group the ROI voxels/vertices such that connectivity is similar for the voxels/vertex within a group and different between groups. That is, distinct clusters are identified in the ROI by differences between long-rang interaction patterns of the voxels/vertices in the ROI. Historically, CBP has first been performed based on whole-brain structural (fiber) connectivity profiles as derived from diffusion magnetic resonance imaging (dMRI) (Behrens et al., 2003; Wiegell et al., 2003). Later, analogous approaches based on resting-state functional connectivity (RSFC) (Kim et al., 2010) and, most recently, meta-analytic connectivity modeling (MACM) (Eickhoff et al., 2011) have been introduced. On the one hand, previous investigations have demonstrated that CBP can reveal clusters that recover known histological parcellations (e.g., Bzdok et al., 2012; Johansen-Berg et al., 2005). On the other hand, there are also reports showing that CBP may yield more fine-grained subdivisions than classical cytoarchitectonic mapping (e.g., Clos et al., 2013). Hence, CBP-derived modules may be viewed as 'functional areas', although these are outlined by connectivity differences rather than function.

The ability of CBP methods to map functional areas led to rapid adoption by neuroimaging investigators (cf. Smith et al., 2013a). Yet, several circumstances encourage heterogeneity in this nascent field. Methodologically, the CBP procedure is based on practical choices inconsistent across laboratories. Importantly, no single package permitting CBP is, to the best of our knowledge, openly distributed at the moment. Rather, it seems that different research groups perform CBP analyses based on their own script library, in-house databases, and laboratory setups. However, sharing of code implementations and international collaboration on its successive improvement will hopefully contribute towards a widely accepted software infrastructure (cf. Pradal et al., 2013).

Challenges that typically arise in CBP studies will be discussed in different sections. We will start out with the purpose of CBP and the neurobiological conclusions that can be drawn from it. The subsequent sections deal with the initial, interrelated decision on the ROI definition and the connectivity aspect to be investigated. We will then outline the main clustering approaches and corresponding cluster-selection criteria. The ensuing CBP results frequently raise questions around statistical inference and double dipping, discussed in later parts of the manuscript. We finally reflect possible ways to capitalize on CBP results as a starting point for multi-modal

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3 studies. All these issues are discussed below by providing overview, potential pitfalls, and possible solutions
4 aimed at neuroimaging novices and experts. We hope that these considerations may ultimately help unify the
5 dynamically developing *spectrum of CBP methods*.
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For Peer Review

I Motivation

1.1 Aim

The principle of brain segregation guided by long-distance connections can be attractive from different perspectives, including the investigation of local functional differentiation, the creation of data-driven brain atlases, and catalyzing the inception of unprecedented hypotheses.

Location mapping. Comparing to other current neuroimaging approaches, CBP has the key strength to actually *map* distinct brain areas. This can be opposed to either localizing a particular (dys)function or characterizing a particular region. Most whole-brain association studies, be it functional MRI, voxel-based morphometry, lesion mapping, or most resting-state connectivity analyses, primarily elucidate *the location* in the brain of a particular effect such as the recruitment by a particular task, a differential response between two conditions, a difference between two groups, or the association with a particular phenotype. They are mapping cognitive, behavioral, and clinical aspects onto the brain. They do however not allow constructing a map from the brain itself (cf. Amunts et al., 2014 for a more detailed discussion). Put different, most neuroscientific methods associating behavior with aspects of neurobiology are naïve to underlying neurobiological compartments. While observing mappings between behavior and the brain, these methods are not well suited to establish or question the architecture of the brain itself (Frackowiak and Markram, 2015). That is, rather than providing a map of the brain, they provide a map of a particular functional or structural feature (such as recruitment by a particular task or aberrations in a particular group of patients) in brain space. The potency of brain-behavior interpretations can however be increased when constrained by knowledge of brain organization units (Devlin and Poldrack, 2007). CBP can propose such organizational units.

Atlas mapping. CBP methods are capable of automatically compartmentalizing the human brain into topographically delineated, functionally distinct regions (Behrens and Johansen-Berg, 2005). That is, 3D brain atlases can be obtained as quantitative models of brain segregation. In that context, an atlas represents a map of (parts of) the brain that assigns each location (voxel/vertex) to a particular structure and hence provides a segregation of the assessed volume into distinct modules. In *whole-brain CBP*, the ROI to be segregated covers the entire gray matter. By evaluating connectivity strengths from each gray-matter voxel/vertex to every other gray-matter voxel/vertex, a compartmental model of functional organization in the cerebral cortex can be derived. In *local CBP*, the ROI to be segregated covers a circumscribed part of gray matter. It can thus be evaluated whether that brain patch contains functionally distinct modules. As another important CBP variant, a-priori hypotheses can be introduced by measuring connectivity only to preselected brain regions, instead of the whole brain (e.g., Behrens et al., 2013; Bach et al., 2011; Sallet et al., 2013). In sum, CBP can readily propose 3D models of brain organization for use as reference atlases.

Hypothesis generation. Many currently employed neuroimaging methods test spatial hypotheses by either localizing effects or characterizing a region, instead of providing explicit hints that encourage novel research hypotheses (cf. Biswal et al., 2010). CBP may be seen as an approach towards the generation of novel hypotheses on regional differentiation. These can subsequently be tested in hypothesis-driven experimental studies. For instance, exploratory CBP evidence supported existence of distinct subregions in the right temporoparietal junction (Mars et al., 2012). This was subsequently confirmed by targeted neuroimaging studies based on cognitive fMRI experiments (Silani et al., 2013), ICA-based experiments (Igelstrom et al., 2015), hypothesis-

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3 driven meta-analysis (Krall et al., 2015), quantitative reviews (Schurz et al., 2014), as well as multivariate
4 pattern analysis in clinical populations (Koster-Hale et al., 2013).
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8 9 *1.2 Neurobiological meaning*

10 What does it actually mean to divide the brain based on differences in connectivity profiles? CBP performs a
11 systematic summary of the Cortex cerebri by combining same tissue and separating different tissue according to
12 an organizational criterion, namely, brain connectivity. Analogous to cytoarchitectonic mapping by
13 microanatomical criteria (cf. Brodmann, 1909, pages 5 and 288-290), functional mapping by connectional
14 criteria critically depends on the certainty that we have about the divisive criterion.
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19 **Cortical areas.** From an anatomical perspective of brain segregation (Amunts et al., 2013), cortical areas are
20 believed to be distinguishable from their neighbors by featuring a distinct (micro)structure, distinct connectivity,
21 and distinct function. In fact, function may follow naturally given that structure and connectivity are thought to
22 conjointly enable *locally specific* neuronal computations (Passingham et al., 2002). As CBP is based on
23 connectivity (true in a strict sense only for dMRI-CBP, cf. below), the defined clusters are not directly
24 interpretable as cortical areas. Note that the current concepts of what constitutes a cortical area are mainly
25 derived from studies of early sensory (Van Essen et al., 1992) and motor (Rizzolatti et al., 1988) brain systems.
26 They may not be readily applicable to higher-level associative brain areas (Yeo et al., 2011), such as the
27 dorsomedial prefrontal cortex (cf. Eickhoff et al., in press). Indeed, with increasing distance from sensory input
28 processing, it is more and more difficult to relate the connectivity pattern of an area to its functional roles (Bzdok
29 et al., 2013a; Bzdok et al., in press; Mesulam 1998; Yeo et al., 2011). Claims about cortical areas based on CBP
30 results may therefore become more and more delicate with increasing level in the cerebral processing hierarchy.
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34 **One single versus multiple parallel subdivisions.** From a more methodological perspective of brain
35 segregation, CBP does not address the neurobiological question whether there is a 'true' parcellation. It is
36 employed to identify the 'optimal' clustering solution, in the sense of best describing the data. It is about the
37 question whether different parcellation results for the same ROI capture different resolutions or dimensions of an
38 underlying neurobiological organization (cf. Kelly et al., 2012; Amunts et al., 2014; Eickhoff and Grefkes 2011).
39 The answer depends on the region of interest. For instance, previous CBP work on the insula (Kelly et al., 2012;
40 Nanetti et al., 2009) and the right temporo-parietal junction (Bzdok et al., 2013b; Mars et al., 2012) have
41 indicated close agreement between the parcellations based on different connectivity modalities. In contrast,
42 parcellations of the posteromedial cortex diverged more strongly between dMRI- and RSFC-CBP studies (Cauda
43 et al., 2010; Zhang and Li, 2012; Zhang et al., 2014). These observations corroborate the relevance of the
44 conceptual differences between aspects of connectivity, such as dMRI, RSFC, and structural covariance.
45 Moreover, there is probably no such thing as *'the connectivity'* for a particular location. There may neither be *'the*
46 *CBP parcellation.'* Rather, brain segregation across connectivity modalities can possibly feature both similarity
47 and dissimilarity.
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51 **Multi-modal comparison.** Unfortunately, there are yet very few studies that address this fundamental question
52 of brain organization. Such a comparison across connectivity modalities is currently impeded by two key factors.
53 On the one hand, results from previous CBP studies are rather inconsistently available to the community as
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3 image files, which renders most attempts to compare findings purely qualitative (Gorgolewski et al., in press).
4 On the other hand, there appears to be a sentiment that a new CBP study in an already analyzed brain region is
5 primarily a replication and hence lacking novelty. This discourages additional work on previously parcellated
6 brain regions.
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10 **Meaning of CBP clusters.** Given the biological and methodological characteristics of the most frequently used
11 anatomical and functional connectivity measures, we would suggest the following tentative distinction. For
12 dMRI-CBP, the delineated clusters most likely reflect truly connectivity-defined modules, even in light of
13 known artifacts (cf. below). In contrast, MACM-CBP reveals clusters that are probably functionally distinct
14 modules even though the spectrum of brain functions is likely to be larger than what can be probed by
15 neuroimaging techniques (cf. Mennes et al., 2013; Smith et al., 2009). That is, task-based functional connectivity
16 might be limited by real-world behavior being richer than in-scanner behavior. The neurobiological nature of
17 RSFC-CBP derived clusters might remain most uncertain. This is because the relation of resting-state
18 correlations to anatomical connectivity, function, and the brain's housekeeping physiology is currently only
19 incompletely understood (Biswal et al., 1995; Zhang and Raichle, 2010).
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26 **The insula.** To take a concrete example, previous CBP results match some neurobiological dimensions of the
27 insula, but certainly not all of them (Fig. 1). On a microanatomical scale, investigations classically divided the
28 insula into a rostroventral (agranular), rostradorsal (dysgranular), and caudal (granular) portions in macaque
29 monkeys (Mesulam and Mufson, 1982a). On a macroanatomical scale, the more rostral insula is preferentially
30 connected to frontal regions, whereas the more caudal insula is preferentially connected to primary and
31 secondary sensory as well as motor regions (Mesulam and Mufson, 1982b; Mufson and Mesulam, 1982a). On a
32 developmental scale, anterior-posterior segregation in the human insula becomes observable within the first two
33 years of life, as indicated by RSFC-CBP in infants (Alcauter et al., 2013). From the perspective of sensory input
34 channels, the insula contains primary gustatory, primary auditory, as well as associative somato- and
35 viscerosensory cortices. On a functional scale, along the caudo-rostral insula, primary interoceptive
36 representation gradually shifts over environmental input representation into highly abstract cognitive
37 representations of self and time (Craig, 2009). These observations exemplify that an identical ROI may be
38 segmented along diverging features and notions of brain organization.
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44 More globally, it appears that agreement across connectivity modalities decreases when the parcellation becomes
45 more fine-grained. In this context, it is important to appreciate that many brain regions may be described at
46 multiple scales and by multiple notions. It is hence likely that there are several correct answers to the question of
47 a neurobiologically valid parcellation, even when based on a single approach. This has probably best been
48 demonstrated for the insula, subject to repeated CBP analyses (Nanetti et al., 2009, Chang et al., 2013, Kelly et
49 al., 2012, Cauda et al., 2012, Deen et al., 2011, Jakob et al., 2011, cf. also Kurth et al., 2010). This previous work
50 has shown that the insula may be described by a primary rostral-caudal distinction (cf. Alcauter et al., 2013) as
51 well as a repeatedly reported a triplet of rostroventral, rostradorsal, and caudal portions. Diverse functional
52 recruitments and more fine-grained parcellation schemes, such as described by Kelly et al. (2012) and Nanetti et
53 al. (2009), should then reflect additional differentiation within these.
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3 **Hierarchical level, functional gradients, and completeness.** Three further aspects that need to be considered in
4 any neurobiological interpretation of CBP results are hierarchical level, functional gradients, and completeness.
5 i) Generally, boundaries between brain regions become less clear with increasing abstraction level in the neural
6 processing hierarchy. This is reflected by the fact that the more similar the connectivity patterns of two areas are,
7 the more difficult it is to demonstrate a functional double dissociation by lesion studies (Young et al., 2000). In a
8 CBP context, particular care and modesty is therefore recommended when investigators interpret functional
9 borders in highly associative brain regions. ii) Both high- and low-level processing regions in the brain may
10 feature dedicated functional gradients. For instance, the left inferior parietal lobe (i.e., a high-level region) might
11 contain a functional gradient from more person-state- to more person-trait-related processing facets in social
12 judgments (Hensel et al., in press), while V1 (i.e., a low-level region) contains functional gradients related to
13 retinotopy ~~and ocular dominance~~ (Wandell et al., 2007). Whenever there is previous evidence for functional
14 gradients in a ROI, investigators should be careful not to overstretch the discovered functional mapping. This is
15 because the commonly used clustering algorithms (e.g., k-means, spectral, and hierarchical clustering) will
16 impose clear-cut boundaries somewhere along such gradual transition zones. iii) It is moreover noteworthy that
17 the distinct functional modules identified in a locally circumscribed ROI might extend beyond the boundaries of
18 that ROI (cf. next section).
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27 Taken together, convergence and divergence across parcellation schemes should raise the attention of CBP
28 investigators. It is conceivable that discussing CBP results exclusively by a single parcellation solution of the
29 ROI might entail loss of neurobiological insight. Investigators should treat diverging parcellation solutions (at
30 same and different cluster numbers) as potentially complementary rather than strictly exclusive. Indeed, the
31 insula did feature several stable parcellation solutions in a dMRI-CBP study (Nanetti et al., 2009). To facilitate
32 more comparison across modalities and CBP approaches, however, the neuroimaging field probably needs
33 increased sharing of CBP parcellations and more complementary investigations of already examined regions
34 using different connectivity measures and approaches. Put differently, connectivity-derived clusters are primarily
35 descriptions of the data. Meaning of clusters can only arise in the adoption of a neurobiological viewpoint. They
36 do not, however, simply represent 'cortical areas'. Hence, this term should probably be avoided until sufficient
37 evidence has been gathered on distinctions from neighboring areas in terms of structural, functional and
38 connectivity-related features. Moreover, clusters in the associative cortices and those identified in regions with
39 evidence for functional or structural gradients need to be interpreted with particular caution.
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II Procedure

2.1 ROI definition

The first decision in CBP analyses is on the part of the brain to analyze. The ROI outlines the set of target gray-matter voxels/vertices that the investigator wishes to segregate into subregions. This important step operationalizes the investigation, which strongly impacts the overall outcome and interpretation of the study.

Whole-brain CBP. As the perhaps most intuitive choice, the ROI may comprise the entire gray matter in the aim of *whole-brain parcellation* (e.g., Craddock et al., 2012; Shen et al., 2013; Thirion et al., 2006b; Thirion et al., 2014; Yeo et al., 2011). A ROI with all voxels/vertices in gray matter can for instance be drawn from the ICBM tissue map (International Consortium on Brain Mapping) at a gray-matter probability of choice (e.g., Bzdok et al., 2013b), from gray-matter segmentation (Fischl et al., 2004), as well as from the MNI (Evans et al., 1992) or Talairach-Tournoux (1988) template spaces. Importantly, it might not always be the most attractive option to group the brain in voxel or vertex units. Single voxels/vertices can hardly be interpreted by themselves (cf. Chumbley & Friston, 2009). Additionally, operating in a voxel/vertex space can make clustering procedures computationally expensive. Rather than *voxel/vertex-level clustering*, whole-brain parcellation lends itself to *node-level clustering*. That is, not individual voxels/vertices but predefined groups of voxels/vertices (i.e., nodes) are the units that are grouped as a function of connective similarity (Smith et al., 2013b). Note that the nodes represent voxel/vertex combinations based on previous knowledge that can, for instance, be derived from ICA or structural atlases. Constructing nodes as an alternative unit of observation is therefore not itself an instance of clustering. An advantage of performing a connectivity-based grouping of nodes covering the brain's gray matter relies in the increased neurobiologically interpretability. This is because these nodes are often created based on neurobiological features, whereas a single voxel/vertex does usually not allow a one-to-one mapping of salient neurobiological properties. For instance, using each region of the default-mode network as nodes allows finding node clusters that represent functionally distinct subnetworks (Andrews-Hanna et al., 2010). Such node definitions can be called *hard* (i.e., one single shape) or *soft* (i.e., several slightly different shapes dependent on occurrence likelihood) (Varoquaux et al., 2013). Concretely, subregions from hard ROI clustering are typically non-overlapping, whereas subregions from soft clusterings can typically be overlapping. Frequently used hard brain nodes include cytoarchitecture (Brodmann, 1909) and AAL (Tzourio-Mazoyer et al., 2002), while frequently used soft brain nodes include the probabilistic atlases from Jülich (microanatomical) and from Harvard-Oxford (macroanatomical). As a more data-driven variant of whole-brain parcellation, sets of coherent functional nodes can be obtained by (spatial) independent component analysis (ICA; Beckmann et al., 2005; Malherbe et al., 2014; cf. below). Yet, note that the optimal conceptualization of a 'node' is unclear and the practical choice is a matter of debate (Zalesky et al., 2010). A whole-brain atlas of functional nodes can also be learned directly from RSFC data of multiple subjects in a probabilistic hierarchical model (Varoquaux et al., 2011). Among whole-brain CBP approaches, one might further distinguish *3D-volume-based parcellation* (most studies cited in this paper) and *surface-based parcellation* (e.g., Yeo et al., 2011; Blumensath et al., 2013; Gordon et al., 2014). Further, whole-brain parcellations, be it based on individual gray-matter voxels/vertices or preset voxel/vertex groups as nodes, enjoy increasing popularity. Whole-brain CBP might be particularly important for current and future high-throughput projects in neuroscience (e.g., the European Human Brain

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3 Project [HBP], the international Human Connectome Project [HCP], the American Brain Research through
4 Advancing Innovative Neurotechnologies [BRAIN]) (a very good overview is given in Poldrack & Gorgolewski,
5 2014).
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9 **Regional CBP.** In contrast to whole-brain CBP, the majority of existing CBP studies used a ROI that outlines a
10 circumscribed part of the brain. The underlying motivation typically relates to a test of functional heterogeneity.
11 Note however that whole-brain CBP provides individual clusters that can each be used as circumscribed ROI.
12 Practically, cluster from whole-brain CBP studies can subsequently serve as targets for local regional CBP
13 studies. One can distinguish between *anatomical* and *functional* ROIs. An anatomical ROI can be constructed in
14 a straightforward fashion by manually outlining macroanatomical landmarks guided by gyri, sulci, ventricle
15 borders, or white matter (e.g., Anwender et al., 2007; Beckmann et al., 2009; Mars et al., 2011; Solano-Castiella
16 et al., 2010). One might note three relevant aspects. First, this type of ROI definition may be limited by the fact
17 that sulcal/gyral boundaries do not always coincide with functional boundaries (Amunts et al., 1999; Zilles et al.,
18 1997; in contrast to Weiner et al., 2014). Intentionally extending the ROI may therefore be an attractive option
19 (cf. below). Second, these gross anatomical features can be subject to considerable inter-individual variability
20 (Kochunov et al., 2010). This encourages region delineation on a single-subject basis. The presence or absence
21 of the paracingulate sulcus may, for instance, not be captured by an automated group-level procedure (cf.
22 Beckmann et al., 2009). Third, manually defined ROIs might be thought of as more subjective by some authors.
23 While the ensuing CBP studies could suffer from poor reproducibility, a completely automatic method is
24 however no guarantee for better results (cf. below). Note that all three presented caveats are controversial in the
25 literature. As a frequently used alternative, macroanatomical ROIs may be based on probabilistic maps such as,
26 e.g., provided by the Harvard-Oxford atlas (<http://fmrib.ox.ac.uk/fsl/>) or constructed by automatic segmentation
27 (Fischl et al., 2004). Both strategies have frequently been employed in previous CBP studies (e.g., Bach et al.,
28 2011). Such maps provide objective and reliable masks reflecting the location of a particular structure in a group
29 of subjects that contrast investigator-guided or hand-drawn ROI definitions. Microanatomical ROIs, in turn,
30 represent an attractive alternative because regional heterogeneity of histological features, such as
31 cytoarchitecture (cf. Amunts and Zilles, 2010), is a likely indicator of regional specialization. Such probabilistic
32 cytoarchitectonic ROIs have already been used for CBP studies (e.g., Bzdok et al., 2012; Johansen-Berg et al.,
33 2005). It is however important to appreciate that cytoarchitectonic areas exhibit often marked inter-individual
34 variability and hence may not map well to the corresponding regions of an individual subject following standard-
35 space alignment. Consequently, the resolution of any CBP analysis can only be as accurate as permitted by the
36 preceding realignment procedures. In summary, when using an anatomical ROI, the ensuing CBP analysis
37 addresses the question whether a particular (macro- or microanatomical) structure contains subregions featuring
38 distinct connectivity. More specifically, CBP performed on microstructural ROIs then yields modules that are
39 defined by a particular structure (due to the ROI definition) and connectivity (due to the CBP logic) and may
40 therefore be more likely to represent actual functional units in the brain.
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54 Contrary to anatomical ROIs, neuroimaging researcher sometimes use alleged neuroanatomical terms to
55 predominately denote a certain *function* rather than a certain *location*. Examples for such ‘pseudo-anatomical’
56 regions that often have a rather coarsely defined or even disputed relationship to structural anatomy would be the
57 ‘fusiform face area’ (cf. Kanwisher et al., 1997), ‘frontal eye field’ (cf. Grosbras et al., 2002), and ‘temporo-
58 parietal junction’ (cf. Mars et al., 2012). When interested in such region, a functionally defined ROI might be the
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3 preferred approach. It is possible to use the results of a single fMRI study. In its simplest form, it could be
4 defined by voxels/vertices activated by one or more fMRI tasks. Yet, the functional definition would be highly
5 specific to the respective experimental setup. A principled approach to create a functional ROI from
6 experimental fMRI that acknowledges inter-subject variability is known as *functional localizers* (Friston et al.,
7 2006; Fox et al., 2009; Saxe et al., 2006). Originally, this approach used a separate neuroimaging experiment
8 performed to constrain both analysis (i.e., increasing sensitivity) and interpretation of the actual study. If inter-
9 subject variability is not of interest, it can be an attractive option to consolidate the location of the functional
10 process of interest by means of quantitative image-based (i.e., using whole-brain activation maps; Dehaene et al.,
11 2003; Schilbach et al., 2008) or coordinate-based (i.e., using peak activation information; Eickhoff et al., 2009;
12 Radua and Mataix-Cols, 2009; Wager et al., 2007) meta-analysis. The resulting ROI would then statistically
13 constrain the most robust location of activation convergence underlying the process of interest across various
14 subjects, study designs, and laboratories. In either case, CBP will address the heterogeneity of connectivity
15 patterns within this functionally defined region. This becomes particularly interesting when ROIs are defined by
16 (partially) overlapping activation blobs from experimental neuroimaging studies (Cieslik et al., 2013) or meta-
17 analyses summarizing different functions (Bzdok et al., 2013b) that are located in closely neighboring yet
18 potentially different locations. In cases where a 'composite' functional ROI is used, CBP allows answering a
19 new type of question: 'Are the different cognitive processes reflected by the different activations or meta-
20 analyses related to the same or different connectivity-defined modules in the human brain?' Note that this is not
21 circular even if CBP always locates subregions in the ROI. This is because cluster validity criteria may provide
22 evidence that all obtained cluster solutions are instable and therefore not neurobiologically meaningful. Such
23 judgments should be weighed against external knowledge. CBP with composite ROIs has hence the potential to
24 reconcile controversies in cognitive neuroscience. For instance, the one-module versus mosaic-modules debate
25 for the temporo-parietal junction (Decety and Lamm, 2007; Mitchell, 2008) has probably been resolved by
26 repeated demonstration of functionally distinct subregions using CBP (Bzdok et al., 2013b; Mars et al., 2012).
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38 **ROI borders.** As an important consideration in CBP studies, the outside borders of the non-whole-brain ROI are
39 not tested or validated. They will hence be taken as borders of the ensuing clusters. A thorough motivation of
40 why and how these outside boundaries are defined is pertinent to any CBP study. In turn, if the localization of a
41 particular module is the primary interest of an investigation, it is advisable to dilate the ROI to include sufficient
42 coverage of the neighboring cortex, allowing for additional clusters around the volume of primary interest. That
43 is, CBP may find all borders of the main regions of interest by including neighboring regions of no or limited
44 interest (cf. Sallet et al., 2013; Muhle-Karbe et al., 2015). In principle, if the ROI extends only a little beyond the
45 ground-truth area(s), only a neglectable amount of noise should be introduced into the cluster estimation. If the
46 ROI extends beyond the ground-truth area(s) to extended parts of areas of no interest, then new clusters (of no
47 interest) emerge that delineate the cluster(s) of interest. As an extreme scenario, if the ROI is incorrectly defined,
48 interpretation of the clustering results becomes challenging to impossible.
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55 In sum, different ways for anatomical or functional definitions of a ROI for CBP have been used and are
56 legitimate. This choice and its operationalization should be well motivated. Generally, population or meta-
57 analysis based ROIs are an alternative to hand-drawn ones or those that are based on a single-subject data (e.g.,
58 AAL). In principle, microanatomical ROI definitions can be preferable to macroanatomical ones. In case of
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3 lacking neuroanatomical consensus for the target region in the literature of interest, a functionally motivated ROI
4 suggests itself. A functional ROI can be constructed from neuroimaging studies or activation convergence
5 quantified by meta-analytic methods. Finally, 'composite' ROIs allow answering the specific question how a
6 particular set of findings relate to regional specialization. Apart from that, if the aim is whole-brain parcellation,
7 voxel/vertex-level CBP does less crucially depend on the ROI definition, while node-level CBP currently suffers
8 from uncertainty about the most biologically valid reduction to network nodes and about methodological biases
9 incurred by node choice (Zalesky et al., 2010). As a consequence, the motivation of the CBP study should be
10 consolidated *before* selecting the preferred ROI. This is because the location and type of ROI explicitly frame
11 the scientific question and motivation underlying a CBP study. Consequently, the initially selected ROI
12 constrains the spectrum of permissible conclusions from the later CBP results. Critically, the decision on the
13 ROI should be taken hand-in-hand with the connectivity data of interest. This is because the underlying
14 neurobiological question should guide methodological choices.

22 23 2.2 Measures of brain connectivity

24 Note that the concepts underlying CBP are not bound to a particular connectivity approach. Any method can be
25 employed that yields a connectivity profile for each voxel/vertex in the ROI. In general, the *anatomical*
26 *connectivity* modality most frequently used for CBP-analyses is dMRI (e.g., Anwander et al., 2007; Behrens et
27 al., 2003; Johansen-Berg et al., 2004). The *functional connectivity* modality in most frequent use is RSFC (e.g.,
28 Cauda et al., 2010; Kim et al., 2010; Zhang and Li, 2012). **It has recently been complemented by MACM (e.g.,**
29 **Bzdok et al., 2012; Eickhoff et al., 2011), which is rapidly gaining usage in the field.** As an alternative to
30 anatomical and functional connectivity, structural covariance (Evans et al., 2013) has been used in a small
31 number of CBP studies (e.g., Kelly et al., 2012; Wang et al., 2014). We do not cover the latter in the interest of
32 simplicity and space. It is important to appreciate that all these measures of connectivity strength reflect
33 drastically different ways to conceive and quantify interneuronal communication between brain regions.
34 Choosing one of them is as important as the ROI selection and has far-reaching implications for the
35 interpretation of the identified clusters. At this point it might be helpful to reiterate *that it is not the individual*
36 *connectivity profiles of the voxels/vertices that drive the parcellation but only the differences between those.*

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45 **DMRI.** *Anatomical connectivity* between brain regions can be measured (or rather approximated) using *diffusion*
46 *magnetic resonance imaging*. It delineates the likelihood of white-matter fiber bundles traced to link brain
47 regions (Johansen-Berg and Rushworth, 2009; Jones, 2008). The number of samples reaching any voxel/vertex
48 in the gray matter or, more frequently, the likelihood of passing through brain white matter then provides the
49 connectivity profile of a particular voxel/vertex or node in the ROI. In fact, in *whole-brain CBP* dMRI is seeded
50 from every gray-matter voxel/vertex. In *local CBP* every voxel/vertex in the circumscribed ROI is a seed, while
51 in *node-level CBP* voxel/vertex groups are seeds (goes for all three connectivity modalities). DMRI tractography
52 is evidently closest to the notion of structural connections. Yet, it does not actually capture axonal connections as
53 classically identified by axonal tracing studies in monkeys (cf. Mesulam, 1976). Caveats of tractography include
54 i) the dominance of large fiber bundles, thus omitting sharply curved or very long fiber bundles, which precludes
55 exhaustive assessment of all connections (Ng et al., 2013; Jbabdi and Behrens, 2013) as well as impaired
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3 detection of ii) poorly myelinated or iii) closely neighboring ('kissing') connections. Finally, *dMRI can neither*
4 *precisely delineate cortical origin nor cortical termination of fiber bundles* (Petrides et al., 2012).
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7 **RSFC.** Alternatively, *functional connectivity* can be measured by *resting-state correlations* under the
8 assumption that the coupling strengths between distant brain regions is measurable by correlation between time
9 series of BOLD signal fluctuations *outside of an experimental context* (Biswal et al., 1995; Buckner et al., 2013;
10 Zhang and Raichle, 2010). It quantifies the correlative relationships between distant brain regions in subjects
11 idling in the MRI scanner. This is possible because interneuronal communication continues and is reflected by
12 ongoing physiological fluctuations in the absence of an experimentally imposed cognitive set, i.e., during natural
13 mind wandering, which can be measured using fMRI (Bzdok & Eickhoff, 2015). While RSFC signals have been
14 shown to recover well-documented axonal connections and functional networks, there is an increasing awareness
15 that much of the observed signal may be influenced, if not distorted, by physiological sources (but see Hipp &
16 Siegel). The ensuing conundrum may challenge the interpretation of brain-behavior relationships discovered by
17 RSFC. Despite initial skepticism, the consistency of RSFC results has been demonstrated repeatedly across
18 subjects, brain scans, time points, and other factors (Damoiseaux et al., 2006; Shehzad et al., 2009). RSFC thus
19 provides proxies of dynamic neuronal interactions that might reflect mixtures of various cognitive processes and
20 physiological factors (Smith et al., 2009; contrasted by Mennes et al., 2013).
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23 **MACM.** *Meta-analytic connectivity-modeling*, in turn, operates under the assumption that *functional*
24 *connectivity* between brain regions should entail reliable coactivation (Toro et al., 2008; Robinson et al., 2010).
25 It quantifies correlative increase/decrease of neural activity in distant brain regions *throughout various*
26 *experimental paradigms*. This connectivity modality capitalizes on the increasing trend for large-scale data
27 aggregation, exemplified by Neurosynth (Yarkoni et al., 2011), BrainMap (Fox and Lancaster, 2002), and
28 NeuroVault (Gorgolewski et al., in press). Caveats of MACM include i) reliance on very sparse activation
29 information (i.e., peak coordinates of significant activation), which might entail missing information and biased
30 sampling, ii) inability of subject-specific connectivity analysis, and iii) inheritance of the limitations from
31 experimental neuroimaging studies. In spite of these limitations, the analysis of coactivation likelihoods
32 represents a complementary approach by focusing on the interactions during the performance of externally
33 purported tasks.
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44 **Commonalities and differences.** Several aspects are of note when choosing between anatomical and functional
45 connectivity modalities in a CBP study. None of the three introduced connectivity modalities provides axonal
46 connectivity in stricto sensu (as gleaned from tracing studies in monkeys). dMRI and RSFC are *task-*
47 *unconstrained* (i.e., *task-independent*) as opposed to *task-constrained* (i.e., *task-dependent*) MACM. While
48 dMRI is a measure of *anatomical* or *structural connectivity* by assessing *white-matter trajectories*, RSFC and
49 MACM identify *temporal coincidence* of *neural signals in gray matter*, that is, functional connectivity. MACM
50 builds on experimental fMRI and PET studies motivated by cognitive theory (i.e., *interventional*, capturing
51 metabolic changes in the brain caused by manipulation of environmental variables), whereas participants simply
52 lie still during RSFC and dMRI measurements (i.e., *observational*, capturing baseline brain features without
53 controlled environmental modulation). It may also be noted that none of these methods can distinguish between
54 involved neurotransmitters (i.e., excitatory versus inhibitory neuronal modulations) or ask whether a connection
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3 is stronger in one direction (i.e., "undirected" connectivity). Moreover, we also need to point out that functional
4 connectivity between two regions may be mediated by a third region. That is, RSFC and MACM (but not dMRI)
5 may be driven by indirect connections. This could however be alleviated by computing partial correlations,
6 which is closer to direct interaction by summarizing conditional independences (Marrelec et al., 2006). In fact,
7 regression-based estimators, such as dictionary learning (Lee et al., 2011), instead of standard clustering
8 approaches, may be more robust to the issue of third-party influences. Additionally, RSFC and MACM are
9 generally more sensitive in delineating existing connections but more prone to false positives, whereas dMRI is
10 generally less sensitive with frequent false negative results (cf. Jbabdi and Behrens, 2013). Contrarily to RSFC
11 and MACM, the accuracy of dMRI tract tracings decreases with the distance between the considered regions.
12 Only dMRI- and RSFC-CBP can be conducted in individual subjects (Anwander et al., 2007; Kim et al., 2010).
13 dMRI- and RSFC-CBP thus enable detecting interindividual differences in regional functional organization,
14 while MACM-CBP inevitably generalizes across various inter-individual variability sources in the sampled
15 subject population. As an important consequence, dMRI and RSFC can readily parcellate individual brains and
16 infer group aggregates based on between-subject variance. Contrarily, MACM is constrained to aggregating
17 group-level statistics from meta-analytic experiment databases. Hence, MACM-CBP may provide information
18 on the functional parcellation of a region of interest across many experiments, which often shows remarkable
19 congruency with parcellations derived from other modalities, but does not allow any individual, subject-specific
20 parcellation. Taken together, dMRI, RSFC, and MACM grasp different features of connective brain
21 organization and imply different limitations and promises.

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29 Anatomical and functional connectivity measures are all equally valid for assessing connectivity strengths to
30 perform CBP. dMRI, RSFC, and MACM all lend themselves to whole-brain, node-level, and local CBP. It is
31 important, however, to remember that they are based on fundamentally different concepts of 'brain connectivity'.
32 Roughly, dMRI is most 'structural/physiological' in nature, whereas MACM is exclusively
33 'functional/psychological.' RSFC, in turn, most likely reflects a mixture of both (with a different set of
34 physiological confounds). These considerations may guide the choice of the employed method when the
35 motivation particularly relates to either functional or anatomical questions. Their different limitations and
36 promises might yield conflicting views on the organization of the ROI, even though first comparative studies
37 show a fairly close convergence (Kelly et al., 2012; Wang et al., 2014). Nevertheless, exploiting distinct
38 connectivity modalities is likely to extend the space of questions that we can ask about functional brain
39 organization.

40 41 42 43 44 45 46 47 48 *2.3 Clustering techniques*

49 Clustering uses a similarity measure to group a set of elements into subsets according to their measured
50 similarity. In CBP, the clustering algorithm groups the voxels/vertices/nodes in the ROI into subsets according to
51 similarity of their connectivity profiles, the heart of any CBP approach. As a result of the so-called '*no free*
52 *lunch*' theorem (Wolpert, 1996), no clustering algorithm performs optimally for all ROIs, types of connectivity
53 information, and study motivations. Rather, methods such as k-means, spectral, and hierarchical clustering have
54 all been frequently employed in CBP studies. While these three clustering algorithms have been used for
55 voxel/vertices-, node-, and whole-brain-level CBP, ICA and boundary detection are popular alternatives for
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3 brain parcellation. We will detail in this section how these algorithms behave in theory and in neuroimaging
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Box 1 about here please

K-means. The probably most popular choice in neuroimaging is *K-means clustering* (Lloyd, 1957; Forgy, 1965; Jain, 2010), a *partitional* approach. It divides a ROI into a preselected number of k non-overlapping clusters (Nanetti et al., 2009). In neuroimaging practice, k-means seems to perform best when the subregions in the ROI are expected to be (i) few in number, (ii) of similar size, and (iii) featuring a roughly spherical shape on spatially correlated voxel/vertex/node-wise connectivity (cf. Jain, 2010). Additionally, k-means clustering will converge in the majority of the cases (i.e., seldom early stopping by the tolerance parameter). In a CBP context, the same connectivity data can describe not only one but several stable solutions in ROI parcellation at the *same* preset k (i.e., low reproducibility), such as observed in the human insula (Nanetti et al., 2009). Consequently, the algorithm is conventionally applied many times since k-means fits idiosyncracies in data that may generalize poorly across subjects. As a first practical consequence, the initialization of the cluster centers (cf. Box 1) can be random (Hartigan and Wong, 1979) or based on prior knowledge (e.g., anatomical properties). As a second practical consequence, the ‘final’ solution can be obtained by an averaging procedure or by selecting the centroids from the best solution (cf. Nanetti et al., 2009). Further, the solutions for different selections of k (i.e., different number of clusters) are independent of each other. Repeating the clustering at different k's does not emulate a hierarchical approach (contrary to hierarchical clustering). That is, the solutions for ROI parcellation at each level (k) are independent of the others, which makes parent-children stratifications possible but by no means necessary. As an attractive k-means variant to address the multi-scale nature of brain organization, investigators can first identify the best fitting k clusters and then test for further separability of each obtained cluster individually (Neubert et al., 2014).

Spectral clustering. One of the first clustering methods in the context of CBP (Johansen-Berg et al., 2004) has been *spectral clustering* (Donath and Hoffman, 1973; von Luxburg, 2007). It can be useful to semi-quantitatively obtain a possible number of clusters by inspection (e.g., Johansen-Berg et al., 2004; Bzdok et al., 2012). Alternatively, when applying an ordinary clustering algorithm, spectral clustering is able to capture clusters that have complicated shape and are discontinuous, yet that are enforced to be roughly equally sized (Craddock et al., 2012; von Luxburg, 2007). Note that the clustering solutions for different cluster numbers are not hierarchically consistent (analogous to k-means, contrary to hierarchical clustering). That is, nestedness of the resulting partitions of the ROI are not methodologically enforced but might still appear as a biological property of the ROI under study. Spatially constrained spectral clustering appears to be stable in capturing connectional similarity features between ROI voxels/vertices/nodes (i.e., high reproducibility). It might however not accurately represent those (i.e., poor model fit, Thirion et al., 2014). In CBP, spectral clustering might be disfavored by some investigators because it strives to enforce simple structure not naturally present in the brain. In particular, as the potentially biggest drawback of spatially constrained spectral clustering, it imposes a strong spatial structure on the data, which thus precludes capturing such structure in the data (Craddock et al., 2012). As

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3 a practical consequence, the more difficult one expects the clusters to separate (e.g., high-level associative brain
4 regions), the more other clustering algorithms should be preferred.

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6 **Hierarchical clustering.** In contrast to the above-mentioned partitional algorithms, *hierarchical clustering*
7 (Johnson, 1967) represents an *agglomerative* (i.e., *bottom-up*) approach that may reveal connectional similarities
8 at various coarseness levels (Eickhoff et al., 2011). Here, each individual voxel initially represents a separate
9 cluster. These are then progressively merged into a hierarchy by always combining the two most similar clusters.
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11 *Divisive* (i.e., *top-down*) hierarchical clustering operates in the opposite direction (start with one cluster, end with
12 one cluster per voxel/vertex), but is seldom used in neuroimaging CBP. The investigator does not need to specify
13 a cluster number because an organizational hierarchy is generated that allows for a functional-connectional
14 multi-level stratification of the ROI. This introduces the advantage of a nested hierarchical solution of ROI
15 parcellations (i.e., enforced parent-children relationships between clustering solutions with different cluster
16 numbers) at the price of large result quantities. There are, however, at least three important drawbacks associated
17 with hierarchical clustering. First, hierarchical clustering is very sensitive to effects in local neighborhoods,
18 which can have a substantial effect on the higher-level solutions in noisy data such as in neuroimaging. Second,
19 the output evidently depends on the investigator-chosen linkage algorithm, i.e., the rules how clusters are
20 combined. This can be remedied by imposing the additional constraint of merging only spatially neighboring
21 clusters, which tends to be better behaved (Thirion et al., 2014). More specifically, as a both biologically
22 plausible and *greedy* (i.e., exploiting computationally convenient simplification) variant, *spatially constrained*
23 *hierarchical clustering* merges/divides only immediately neighboring clusters. Unfortunately, different linkage
24 algorithms tend to yield different solutions. Finally, there is a tendency for (non-spatially constrained)
25 hierarchical clustering to yield very imbalanced cluster sizes. In the extreme case, one after one
26 voxel/vertex/node is added to a group containing all other ones. This clustering algorithm should be preferred
27 when expecting many clusters (contrarily to k-means). Depending on the merging heuristic, it can however be
28 quite computationally expensive (e.g., complete clustering). Hierarchical clustering captures well the properties
29 of the connectivity differences (i.e., high accuracy) but its solutions may be inconsistent (i.e., low
30 reproducibility, like k-means). As a rule of thumb, accuracy and reproducibility tend to be mutually exclusive
31 across clustering algorithms.
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42 **Distance measures & linkage algorithms.** We would like to emphasize that neuroimaging data are typically
43 noisy (due to intersubject variability, technical limits, etc.) and smooth (due to Gaussian filtering). Consequently,
44 standard k-means, spectral, and hierarchical clustering often find spatially contiguous clusters, although this is
45 not immanent in the respective algorithms. While these considerations take place in the *brain space*, it is
46 important not to confuse it with the *feature space*. Distance in brain space pertains to the spatial spacing (in, e.g.,
47 mm or voxels) between the units to be clustered, whereas distance in feature space pertains to abstract similarity
48 metrics between connectivity measurements. The process of combining voxels/vertices/nodes in the ROI to
49 connectionally homogeneous clusters (i.e., operating in brain space) is strongly influenced by the employed
50 distance measure and linkage algorithm (i.e., operating in feature space) (Hastie et al., 2011). On the one hand,
51 *distance measures* represent the similarity criterion for pairs of connectivity profiles (cf. Jain et al., 2010; Handl
52 et al., 2005). These include the a) Euclidean distance (i.e., squared difference between respective connectivity
53 values; a special case of Minkowski metric at $p=2$), b) correlation distance (i.e., Pearson's correlation of the
54 connectivity profile vectors), and c) cosine distance (i.e., one minus the cosine of the included angle between
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connectivity profile items, acts as normalization). For cosine distance, subtraction of the coefficient from 1 yields a proper distance metric. It can be advantageous in the presence of outliers. If the connectivity data are known to be particularly noisy. It can be advantageous to use cosine/correlation distances or ranked variants of the above distances (i.e., by using Spearman's rather than Pearson's correlation) to improve resistance to outliers. One the other hand, the *linkage algorithm* guides how the measured distances are used to evolve clusters (cf. Stanberry et al., 2003; Timm 2002). The linkage dictates how voxels are combined to clusters based on the computed distance measures. It can be a) 'weighted' (weighting average distances, defined in various ways in the literature), b) 'average' (not weighting average distances; mean between all connectivity values in a first cluster to all connectivity values in a second cluster), and c) 'ward' (replaces distance measures to the minimization of intracluster variance) as well as d) 'single' (i.e., shortest distance, often produces a skewed solutions, i.e., 'chaining phenomenon by always adding the respective next closest element with heterogeneous overall clusters), and e) 'complete' (maximum distance, tends towards compact clusters, less preferred for noisy data). The best linkage method obviously depends on the data properties. Some combinations of distance measure and linkage seem to be better than others. For instance, when using Euclidean distance the ward linkage seems robust to outliers in noisy data. For different distance/linkage choices, the hierarchical clusters can also find spatially contiguous clusters at a similar rate as k-means.

Alternative clustering procedures. While k-means, spectral, and hierarchical clustering algorithms are used in various parcellation scenarios, ICA and boundary detection serve very similar goals in whole-brain parcellation. ICA is an iterative, non-closed-form solution to blind source separation (Hyvarinen, 1999). Applied to fMRI data, it is known to separate out stable, statistically independent, and possibly overlapping spatial activation patterns. Note that the time courses of the nodes of each extracted brain 'network' are identical (Beckmann et al., 2005; Smith et al., 2009). As a first conceptual point, this makes ICA a viable instance of connectivity-based parcellation of functional brain imaging data. As a second conceptual point, ICA is an instance of soft clustering by allowing solutions of spatially overlapping clusters (contrarily to the three clustering algorithms above). ICA is special in computing generative models of the signal, it may be more noise-sensitive than the above hard clustering algorithms (Smith et al., 2013a), and allows extraction of artifactual patterns from the data (assuming additivity), not possible with the above clustering algorithms or border detection. Such continuous and probabilistic, rather than discrete and binary, clusters also result from different alternative clustering methods in neuroimaging, including multi-subject dictionary learning (Varoquaux et al., 2013), fuzzy C-means clustering (e.g., Cauda et al., 2010), deep neural networks (Bengio, 2009; Plis et al., 2014), and Gaussian mixture models (e.g., Shen et al., 2010). They share the advantage of extracting stratifications of overlapping patterns. This has limited gain in parcellating ROIs that cover one or very few cortical areas but will be particularly relevant in whole-brain CBP. Indeed, the neurobiological justification for CBP is the connectional homogeneity of individual cortical areas. Yet, soft clustering approaches can flexibly represent overlapping neurobiological clusters with more expressive parcellation models (cf. Passingham et al., 2002). Boundary mapping, on the other hand, reconceptualizes clustering as the identification of transitions between territories of adjacent brain areas (Cohen et al., 2008; Wig et al., 2013; Wig et al., 2014). High confidence in boundaries (i.e., high 'edge probability') indicates good cluster separability, and vice versa. Detected boundaries are interpreted as localized, abrupt changes in connectivity profiles. Boundary mapping has been instrumental in segregating both circumscribed brain regions (e.g., frontal cortex, Cohen et al., 2008; lateral parietal cortex, Nelson et al., 2010)

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3 and the entire brain (e.g., Wig et al., 2014). Given the possibility of generating probability boundary maps (e.g.,
4 by Canny edge detection algorithm), edge modeling qualifies as a mixture between hard and soft clustering. All
5 clustering procedures mentioned up to this point can be applied in single-subject and group analysis.
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9 More globally, each time the investigator chooses a clustering algorithm to be applied on the ROI, he or she
10 accepts a number of implicit or explicit assumptions (Hastie et al., 2011). Therefore, *any clustering algorithm*
11 *unavoidably biases the resulting clustering solution with respect to the number, shape, relative sizes, hierarchy,*
12 *and contiguity of the clusters.* Consequently, investigators should resist the temptation to promote their CBP
13 study as 'completely model-free', 'purely data-driven', or 'without any assumptions.' Rather, it is important to
14 realize the inevitable assumptions and biases of a clustering algorithm and motivate the choice of a particular one
15 based on the aim of the study, the ROI, and the employed connectivity data (Handl et al., 2005). Moreover, using
16 different connectional modalities and other imaging modalities, the investigator can provide a valuable cross-
17 confirmation of the clusters' biological relevance. Cross-species evidence in favor of a parcellation solution
18 might be especially important (cf. Ramnani et al., 2006; Sallet et al., 2013; Neubert et al., 2014).
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28 **Inferential versus exploratory statistics.** In short, assessing the significance of brain parcellation results is
29 hard. This is particularly true if *significant* is employed in the strict sense of inferential statistics and not
30 employed in its broader sense of 'interesting' or 'relevant.' The key problem in wanting to assess statistical
31 significance of CBP results is the requirement of a *null hypothesis* to test against. Conceptually, a ROI clustering
32 solution would hence be deemed *statistically significant* if it has a very low probability of being true under the
33 null hypothesis that the investigator seeks to reject. Yet, such a null hypothesis is often difficult to formulate in
34 clustering applications. Instead of *inferential statistics*, which *test for a particular structure* in the clustering
35 results, investigators need to resort to *exploratory statistics*, which *discover and assess structure* in the data
36 (Efron and Tibshirani, 1991; Tukey, 1962; Hastie et al., 2011). While it is true that statistical methods span a
37 continuum between the two poles of inferential and exploratory statistics, comparing the 'importance' or
38 'pertinence' of clustering results from a CBP analysis is naturally situated more towards the latter. CBP hence
39 represents an unsupervised statistical learning problem that is conventionally addressed by quantitatively
40 comparing *model fit* using *cluster validity criteria*. It may therefore be seen as one instance of a current shift in
41 neuroimaging away from classical inferential towards exploratory approaches, put differently, from
42 voxel/vertex-level mappings to more global assessment of model fit or predictive power (cf. Brodersen, 2009;
43 Cox and Savoy, 2003; Naselaris et al, 2011).
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52 **Cluster validity problem.** From a broader perspective, the 'true' shape and number of clusters is unknown for
53 most real-world clustering problems, including brain research. Finding an 'optimal' number of clusters represents
54 an unresolved issue (*cluster validity problem*) in computer science, pattern recognition, and machine learning
55 (Handl et al., 2005; Jain et al., 1999). This has prompted the development of diverse *heuristics (cluster validity*
56 *criteria)* to weigh the quality of the obtained clustering solutions. These are necessary because *clustering*
57 *algorithms will always find subregions in the investigator's ROI, whether these truly exist in nature or not.*
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3 **Cluster separation criteria.** Criteria can be based on the separation between clusters such as the silhouette
4 value (which for each element measures how similar that element is to the other ones in its own cluster, when
5 compared to the nearest clusters) or the inter/intra-cluster distance (which compares the distance between the
6 cluster-centers to the distance between the elements within each cluster). Such criteria reflect the goal of CBP,
7 i.e., to form groups such that voxels/vertices/nodes within a group show similar connectivity, while the
8 connectivity is different between groups. Note however that *successively segregating brain connectivity data*
9 *into clusters tends to result in lower within-cluster and higher between-cluster differences in ever step,*
10 *regardless of the applied clustering algorithm and the chosen cluster validity criterion.*

14 **Consistence across parcellations.** Criteria can also be based on the consistency across parcellations into a given
15 number of clusters. This set of criteria comprises metrics, including variation of information (VI), the Dice
16 coefficient, normalized (NMI) or adjusted (AMI) mutual information as well as *adjusted Rand index* (ARI).
17 These kinds of criteria are often used in multi-subject, possibly also within-subject, settings. That is, when a
18 given ROI is parcellated separately in each subject based on dMRI or RSFC information (not possible with
19 MACM-CBP). In such studies, assessing the quality of a particular clustering solution by testing the consistency
20 across subjects has emerged as an important standard. Nevertheless, the same concept has also been applied to
21 test consistency across parameters such as filter size or to evaluate the stability based on procedures such as
22 bootstrapping (i.e., summarizing statistical results across analyses of resampled data drawn with replacement
23 from the dataset; Efron & Tibshirani, 1994).

28 **Consistence across cluster numbers.** Criteria can be based on the hierarchical consistency, such as the VI
29 across clustering solutions (e.g., how different is the information contained in a 4-cluster as compared to a 3-
30 cluster solution) or the hierarchy index (what is the proportion of voxels/vertices/nodes that are originating from
31 the dominant parent cluster). These metrics are only useful in the context of non-hierarchical clustering
32 algorithms, such as spectral and in particular k-means clustering, as hierarchical clustering inevitably yields a
33 perfect hierarchical consistency.

36 **External knowledge.** Criteria reflecting convergence of the different cluster solutions with independent,
37 external information, such as CBP performed in other data modalities or a priori anatomical/functional
38 knowledge, finally, represent a very distinct class of criteria (Handl et al., 2005; Jain et al., 2010). On the one
39 hand, they are, in contrast to the aforementioned metrics, independent from the actual data and hence provide
40 external validity. On the other hand, they are based on the problematic assumption (cf. Amunts et al., 2014) that
41 different sources of information should yield the same parcellation of the brain. This has repeatedly been
42 challenged and in fact can result in a strong confirmatory bias.

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In sum, the desire to test the 'statistical significance' of a clustering solution is hard to fulfill (cf. Breiman, 2001;
Vogelstein et al., 2014). The wish to assess the 'trueness' of clusters within (i.e., cluster comparison) or between
(i.e., model comparison) a cluster number choice may be a more legitimate concern. Choosing the clustering
solution with the highest model fit represents an unsupervised statistical learning problem that cannot be easily

framed within the realms of inferential statistics (Jain, 2010). Rather than trying to test whether a clustering solution reaches *statistical significance*, we propose assessing different *cluster validity criteria* to choose among CBP results. More than one single cluster validity criterion should be used because *the choice of one objective cluster validity criterion is still a subjective choice by the investigator*. We would therefore suggest guiding the choice of a final parcellation by majority vote across a number of complementary cluster validity criteria. These evaluate the more or less good model fit of a given clustering solution in the sense of explaining the data. Even more so, an informed and confident decision on the most pertinent ROI segregation should be justified by consistency across different clustering algorithms and cluster validity criteria (Clos et al., 2013). More generally, the neurobiological 'ground truth', unknown to us neuroscientists, is probably hierarchical, modular, and multi-scale (Frackowiak and Markram, 2015).

Table 1: Main characteristics of cluster validity criteria in brain parcellation

Cluster validity criterion	Rationale	Used in previous brain parcellation studies
Across-subject consistency	finds the number of clusters that yields the highest similarity across independent analyses in a number of subjects; this can be done for instance in a cross-validation framework (e.g., leave-one-subject out) or by a split-group approach	Buckner et al., 2011; Liu et al., 2013; Saygin et al., 2011; Solano-Castiella et al., 2010
Across-hemisphere symmetry	computes the percentage of cluster assignments that agree in both hemispheres; can evidently only be performed in paired brain regions outside of the midline	Bzdok et al., 2012; Kahnt et al., 2012
Adjusted Mutual information (MAI)	assesses the similarity between i) the joint distribution of two sets A and B and ii) the marginal distributions of these two sets; it thus weighs how much information is shared between A and B; results in 0 if A and B are independent, in 1 if they are deterministically related; 'adjusted' implies correction for agreement between clusters out of chance (=RAI); it accounts for the fact that the MI is generally higher for two clustering solutions with a larger number of clusters, regardless of whether there is actually more information shared; related to VI	Thirion et al., 2014

Adjusted Rand index (RAI)	in analogy to mutual information, a measure from probability theory to assess the statistical dependence between two clustering solutions; Rand index is a measure of accuracy between two clusterings; 'adjusted' implies the corrected-for-chance variant of the Rand index (cf. MAI); RAI can be an order of magnitude faster than AMI	Thirion et al., 2014
Akaike's information criterion (AIC)	derived from information theory, it finds the best number of clusters by acknowledging the trade-off between goodness-of-fit and model complexity (i.e., number of clusters); it is based on a probabilistic model and a measure of complexity; this penalty for the cluster numbers is aimed at preventing overfitting, yet is independent of the sample size; as it is a relative measure, it judges the absolute quality of the finally selected model	Zalesky et al., 2010
Bayesian information criterion (BIC)	despite many similarities to AIC, BIC is motivated by a Bayesian approach to model selection; it penalizes the model complexity (i.e., number of clusters, =AIC); in comparison to AIC, BIC imposes higher costs on more complex models (i.e., small cluster numbers are privileged)	Thirion et al., 2014
Cramér's V	assesses the statistical correlation between two groups of discrete values (i.e., voxel/vertex/node-wise cluster assignments) based on chi-square; put differently, it measures the strength of association between two clustering solutions	Liu et al., 2013; Solano-Castiella et al., 2011
Dice coefficient	assesses the similarity between two samples or adjacency matrices; primarily practically justified rather than backed up theoretically; works well in heterogeneous and outlier-prone data; can be used to compare group and single-subject clusterings; can be computed in different ways; it is equivalent to the <i>Jaccard index</i> because there is a monotonic transformation between their scores	Blumensath et al., 2013; Craddock et al., 2012; Shen et al., 2013; Wang et al., 2014
Inter- versus intra-cluster distance ratio	assesses cluster separation by the ratio between the average distance of a voxel/vertex/nodes to its cluster centre and the average distance between the cluster centres; a significantly increased ratio compared to the K-1 solution would indicate a better separation of the obtained clusters	Bzdok et al., 2014; Chang et al., 2009
Percentage of misclassification	assesses cluster assignment by the amount of noise and potentially local effects in the clustering; the average percentage of voxels/vertices/nodes that were assigned to a different cluster compared to the most frequent assignment of these	Bzdok et al., 2014

	voxels/vertices/nodes; used to compared ways to compute a same or different number of clusters	
Percentage of parent-children congruency	assesses cluster topology by how many voxels/vertices/nodes are not related to the dominant parent cluster compared to the solution with K - 1 clusters; counts voxels/vertices/nodes that do not reflect a hierarchical organization; related to hierarchy index	Clos et al., 2013; Eickhoff et al., in press; Kahnt et al., 2012
Silhouette coefficient	assesses cluster separation by measuring how similar that voxel/vertex/nodes is to voxels/vertices/nodes in its own cluster compared to voxels/vertices/nodes in the nearest cluster; good solutions are those with a higher silhouette value compared to the K-1 solution; this measure of cluster quality is independent of the number of clusters	Bzdok et al., 2014; Craddock et al., 2012; Eickhoff et al., in press; Kannan et al., 2010; Zhang et al., 2011
Variation of information (VI)	assesses how much knowing the cluster assignment for an item in clustering X reduces the uncertainty about the item's cluster in clustering Y; a linear expression involving mutual information and entropy; is not adjusted for chance (contrary to AMI and ARI); used to compare ways to obtain a same or different number of clusters	Bzdok et al., 2014; Clos et al., 2013; Eickhoff et al., in press; Kahnt et al., 2012; Kelly et al., 2010

See also http://en.wikipedia.org/wiki/Cluster_analysis.

III Integration

3.1 Claims of circularity

Following ROI parcellation, one of the most frequent questions is what features actually drove this distinction. In other words, ‘what is the difference in connectivity between the identified clusters?’ Thus, the obtained clusters are frequently submitted to supplementary analyses that usually assess the *same* connectivity modality that was initially used to identify the clusters. This kind of follow-up analysis has repeatedly raised the suspicion of circular analysis or *double dipping*.

Double dipping. In neuroimaging, this often refers to the practice of first correlating a behavioral measure with brain activity and then using a hereby identified subset of voxels/vertices for the second ‘actual’ correlation analysis with the same behavioral measure (Vul et al., 2008). Such ‘spurious correlations’ do entail overly enthusiastic results as voxels/vertices have been selected twice for the same purpose in a nested, non-independent fashion (Lieberman et al., 2009). More generally, any statistical analysis has been argued to be invalid when the same data is used for selection and then for discriminative analysis if the test statistic depends on the selection criterion (Kriegeskorte et al., 2009).

Is it an instance of double dipping to use the same (connectivity) data to first identify clusters in a ROI and then compute the connectivity profile of the ensuing clusters? We would argue that it is not. While the clustering step takes place in an exploratory statistical framework, aimed at identifying groups within the ROI voxels/vertices that are similar to each other, the characterization step takes place in an inferential statistics framework, aimed at identifying which target voxels/vertices in the brain have above-chance connections to the clusters (null hypothesis: no part of the brain is connected to the current cluster more than by chance). Put differently, the first step discovers structure in the ROI according to voxel/vertex-wise connectivity, whereas the second step explicitly tests this structure by asking which parts of the brain are significantly connected to the ensuing clusters. As a remark, we can however not test whether two derived clusters have different connectivity. This is because it is connectional differences that led to emergence of these clusters. Put differently, the validity of the statistical test depends on the validity of the underlying null hypothesis. A first way to argue against circularity in this scenario would therefore be that the underlying statistical framework/question of both analyses are markedly different.

Descriptive follow-up analyses. Apart from that, there is a completely different and probably much more pragmatic line of argumentation against accusations of circular analysis. The investigator can explicitly frame the cluster connectivity analysis (i.e., second step) as a *non-inferential* and thus *descriptive* follow-up analysis. This would purely serve to ‘illustrate which are the strongest connectivity differences that contributed to the cluster formation.’ They hence should be considered nothing more than a visualization of what differences caused the cluster formation. Note that this weakens the conclusions on the cluster connectivity results. Nevertheless, purely descriptive cluster characterizations can provide very useful representations of the ROI at hand (e.g., Thirion et al., 2006a; Smith et al., 2013a).

Even if some investigators might be inclined to reproach the post-hoc characterization of connectivity-derived

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3 clusters with circular analysis, it does not appear to hold for connectivity analyses of individual clusters. On the
4 contrary, a comprehensive multi-modal characterization of the obtained clusters in the ROI is strongly
5 recommended. Using the same connectional modality, connectional patterns that drove the parcellation can
6 actually be made explicit in a non-circular fashion.
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10 11 12 3.2 Connectivity-derived clusters as priors

13 **CBP for other analyses.** CBP can yield reliable cornerstones for a variety of consecutive neuroimaging
14 analyses. Experimental methods requiring a-priori target regions can capitalize on CBP clusters to further
15 characterize their behavioral implications by diverse viewpoints towards cross-modal functional mapping. This
16 might include but is not exclusive to transcranial magnetic stimulation (TMS), voxel-based morphometry
17 (VBM), structural equation models (SEM), Granger causality mapping (GCM), and seed-based experimental
18 fMRI analyses. From a broader perspective, CBP has the potential to enhance any neuroimaging technique
19 reliant on prospective region definitions that critically hinges on proper fit of the topographical priors.
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23 **Create atlases as references.** The mentioned methods are not only suited for the creation of spatial maps, but
24 for the characterization of known functional segregation. Connectivity-derived clusters can however be seen as
25 novel, potentially untested hypotheses on regional differentiation. These can be tested in hypothesis-driven
26 experimental studies (i.e., anatomical or functional hypotheses operationalized by region definitions). Asking
27 questions on, for instance, the differences in coactivation pattern of dMRI-defined clusters, the relationship
28 between the regional volumes of the identified regions and phenotypical traits in larger samples or the
29 differential affection of a newly described subdivision in clinical samples are all exciting questions. The
30 information gained from these investigations would then provide a detailed and continuously growing
31 characterization of a brain region within the spatial framework of a particular CBP differentiation. A map of
32 functionally distinct subregions might also serve as an independent reference to explain closely neighboring but
33 topographically diverging activation clusters in task-based experimental neuroimaging studies (e.g., Decety &
34 Lamm, 2007; Cieslik et al., 2013), for the characterization of hemodynamic response profiles (Ciuciu et al.,
35 2003), as well as for functional connectome applications (Smith et al., 2013a; Varoquaux & Craddock, 2013).
36 CBP may thus serve as a *post-hoc analysis* to complement interpretation and as a *preceding analysis* to inform
37 the design of experimental neuroimaging investigations.
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46 CBP may therefore fill a vacuum in the current research landscape in providing new spatial maps of brain
47 regions (i.e., *discovering structure in the brain*). These can then be further characterized by a multi-modal
48 investigation of the (differential) structure, connectivity, and function as well as their relation to various
49 phenotypes in health and disease (i.e., *testing structure in the brain*). Moreover, CBP could become a crucial
50 preliminary step to improve the potency of various seed-based neuroimaging methods.
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55 **Conclusion**

56 Connectivity-based parcellation is currently one of the most exciting yet also one of the most fluidly evolving
57 approaches in neuroimaging research. In contrast to most existing methods, it may yield maps of the brain that
58 can be seen as spatial hypotheses on functional or structural segregation – a hypothesis that may and should be
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3 tested by integrative, multi-modal investigations. We hope, however, that this overview has also raised
4 awareness for the various pitfalls that may be encountered when performing or reviewing CBP analyses; from
5 the initial definition of the ROI (which operationalizes the motivation for that particular investigation and
6 constrains all conclusions that can be drawn), to the choice of the clustering algorithm (with each having its
7 specific strengths and biases), cluster number (which should be based on the examination of multiple metrics and
8 with awareness for multi-level biological organization), and finally the difficulty to apply classical inferential
9 statistics in the context of CBP. Brain parcellation not only serves the generation of new hypotheses. Rather, it
10 might allow new insight into the principles of regional organization when conducting CBP based on different
11 aspects of inter-neuronal communication. Such multi-modal comparison, hand-in-hand with results from
12 hypothesis-testing approaches, might provide unprecedented insight into the organization of regional
13 specialization in human brain's structure, connectivity, and function. Ultimately, connectivity-based parcellation
14 methods offer useful simplified views on brain regions that remain complex in nature.
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For Peer Review

Figure Captions

Figure 1

Different functional segregation models of the insula

From upper to lower panel: a) depicts a concept of functional segregation in the insula as inferred from connectivity studies by axonal tracing in monkeys (Mesulam & Mufson, 1982b), b) two-cluster solution of the maturing insula from connectivity-based parcellation of newborn and two-year-old humans based on longitudinal resting-state measurements (Alcauter et al., 2013), c) three-cluster solution of the insula of human adults shows subdivision of the anterior insula into ventral and dorsal subregions based on resting-state correlations (Deen et al., 2011), and d) different consensus-cluster solutions of the right and left insula in human adults based on the three connectivity modalities resting-state correlations, task-derived coactivations, and structural covariance (Kelly et al., 2012).

Box 1

Synopsis of clustering algorithms used for CBP

K-means clustering

Clustering depends on free parameters, including i) the cluster initialization, ii) the cluster number k , and iii) the tolerance for iteration stopping. Initially k voxels/vertices in the ROI are randomly chosen to represent the centers of the k desired clusters. Two steps are then iterated multiple times. First, the ROI voxels/vertices/nodes are assigned to the closest cluster center (i.e., 'centroid'), which equates with partitioning the ROI into k clusters. Second, the k cluster centers are recomputed. As soon as the center needs to be shifted by less than the preset distance threshold (early stopping is often needed for the sake of time), the iterative process stops. Note that the final assignments of ROI voxels/vertices/nodes to particular clusters may vary with different cluster initializations and yield non-optimal solutions at local minima. The same connectivity data may thus result in several stable solutions for the ROI parcellation at the *same* preset k (i.e., low reproducibility), as shown, for instance, in the human insula (Nanetti et al., 2009). Consequently, the algorithm is usually repeated many times.

Spectral clustering

It is based on a similarity matrix quantifying the similarity of the connectivity profiles between any pair of voxels/vertices/nodes within the ROI. The first eigenvectors of the (normalized) Laplacian of the similarity matrix are computed. Those then enable transformation into an alternative data representation in a space with reduced dimensionality as the eigenvectors 'summarize' features of the similarity matrix. The output of this *data transformation* can then be used for either i) *spectral reordering* or ii) an ordinary clustering algorithm. Spectral reordering uses the reduced similarity information to reorder the similarity matrix in such manner that voxels/vertices/nodes that are similar to each other are grouped together (Barnard et al., 1995). This can be useful to semi-quantitatively obtain a possible number of clusters by eye inspection (e.g., Johansen-Berg et al., 2004; Bzdok et al., 2012). Note that hierarchical consistency across solutions for different cluster numbers is not methodologically enforced. That is, voxels/vertices/nodes may be assigned to a different cluster when looking for instance at the clustering solutions with 3 or 4 clusters.

Hierarchical clustering

Each individual voxel/vertex/node initially represents a separate cluster. These are then progressively merged into a hierarchy by a) always combining the two most similar clusters (i.e., bottom-up) or b) always dividing the least homogenous cluster (i.e., top-down) in every step. The algorithm implicitly walks through different choices of cluster numbers as these approaches generate a hierarchy that allows for a nested multi-level parcellation of

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3 the ROI, even if only few of those are interpreted in practice. Such successive clustering trees introduce the
4 advantage of a nested hierarchical solution of ROI parcellations (i.e., enforced parent-children relationships
5 between clustering solutions with different cluster numbers) at the price of large result quantities. Even if this
6 clustering model reflects current views on the hierarchical organization of the brain, a given hierarchical
7 clustering result is not necessarily neurobiologically valid.
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